

MACHINE
VISION
GROUP

Multi-modality Medical Image Registration

Peter Rogelj, Ph.D.

Faculty of Electrical Engineering,
University of Ljubljana, Slovenia



Contents

- ♦ **Introduction**
- ♦ **Image registration process (optimization)**
- ♦ **Similarity metrics**
- ♦ **Geometric models**
- ♦ **Examples**



Introduction

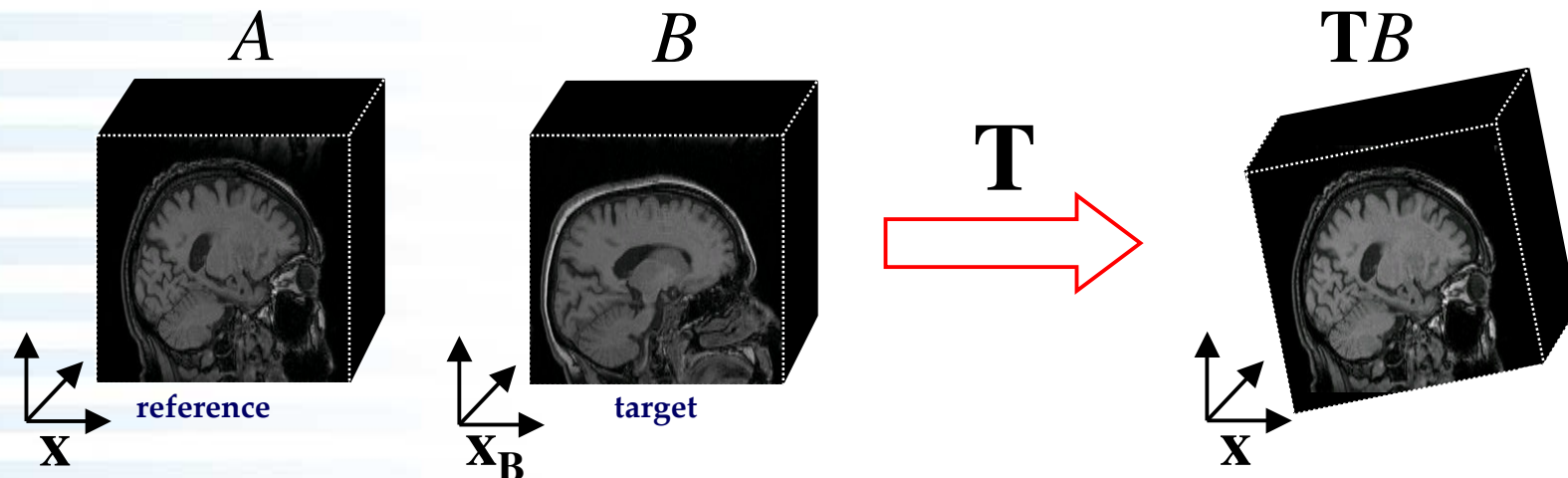
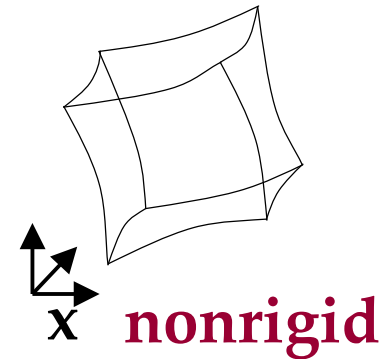
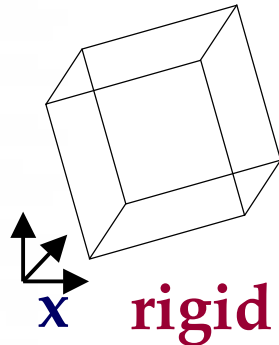


Image registration is a process of finding optimal geometric transformation (T) that puts two images into spatial correspondence.

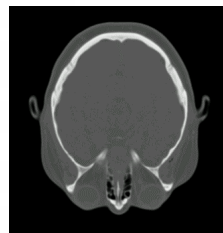


Classification

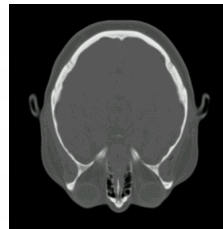
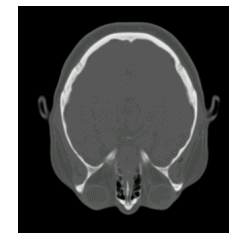
Rigidity:



Modality:



mono-modality



multy-modality



Features:

geometric / intensity

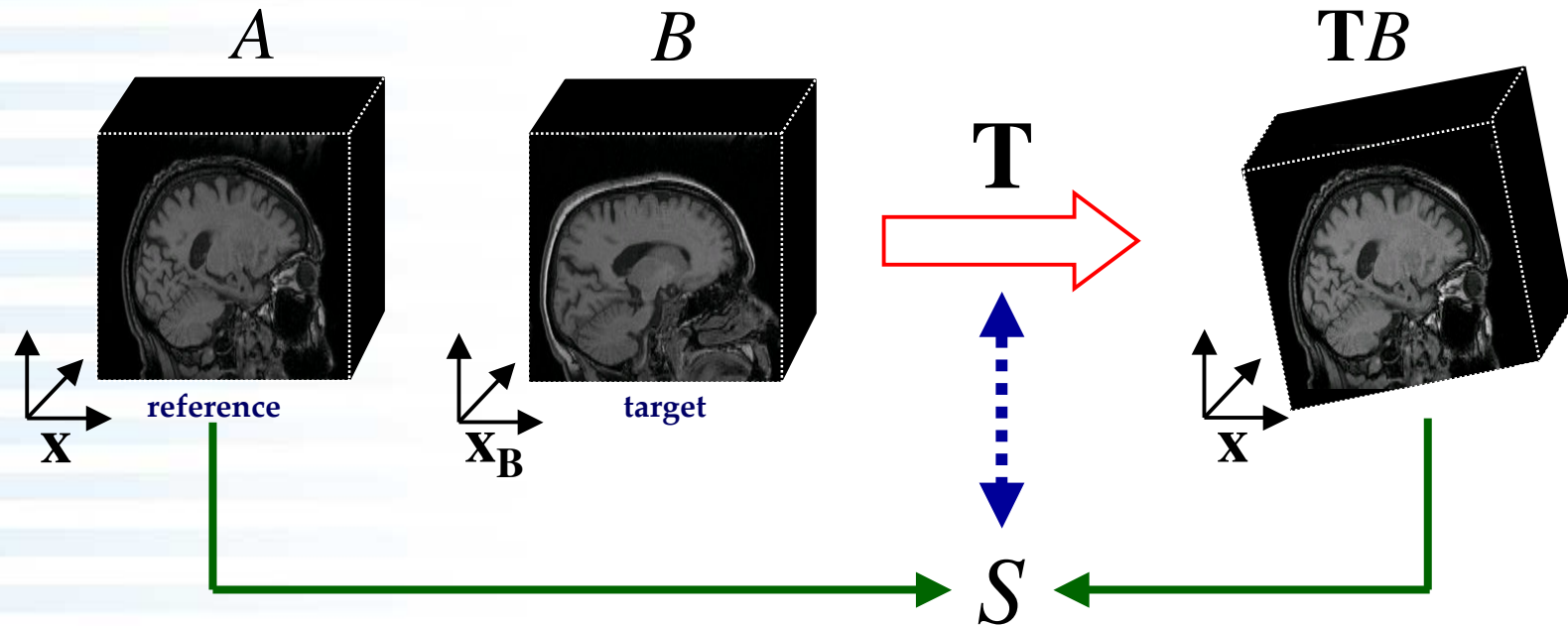


Applications

- ♦ **Image information analysis**
 - ♦ image comparison
 - ♦ image fusion
- ♦ **Image geometry analysis**
 - ♦ analysis of tissue deformation
 - ♦ analysis of organ activity
- ♦ **Image segmentation**
 - ♦ Image to atlas registration



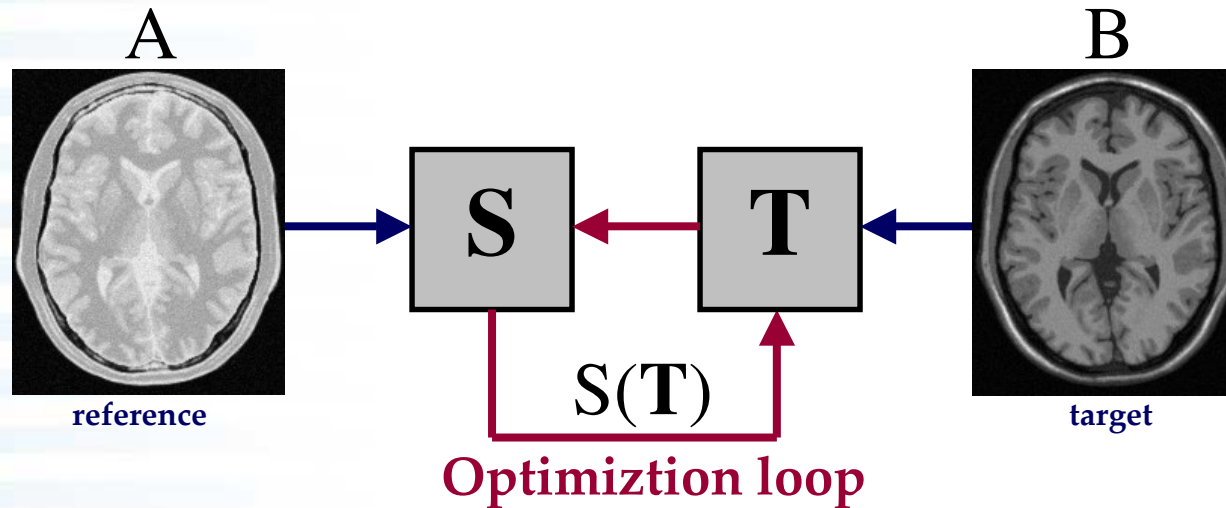
Approach



Registration is an optimization **process** of finding such **transformation** that maximizes **image similarity** (considering geometric limitations of spatial deformation model).



Parametric reg. process



Global: 3D rigid: 6 parameters

3D affine: 12 parameters

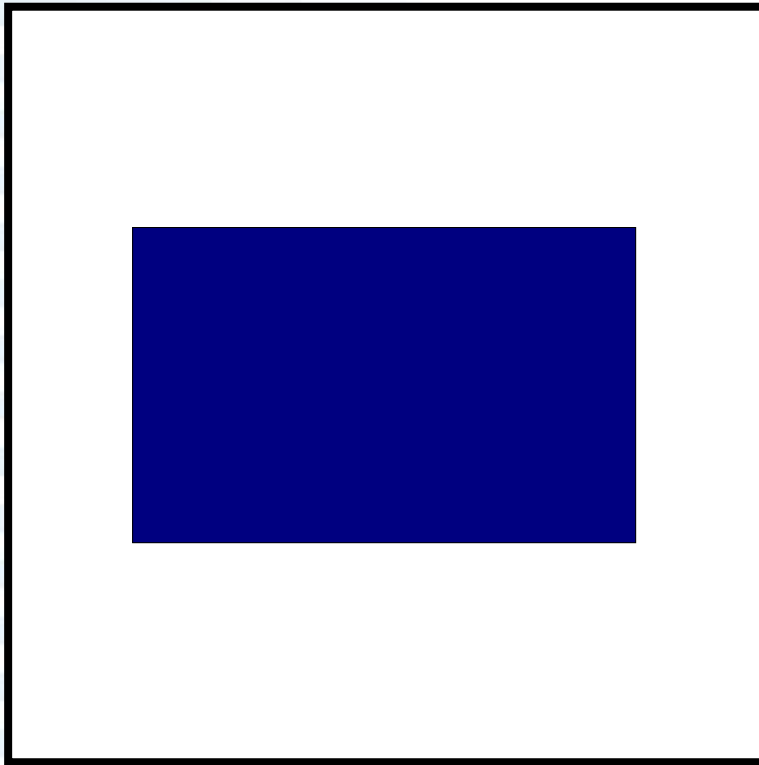
...

Local: splines...

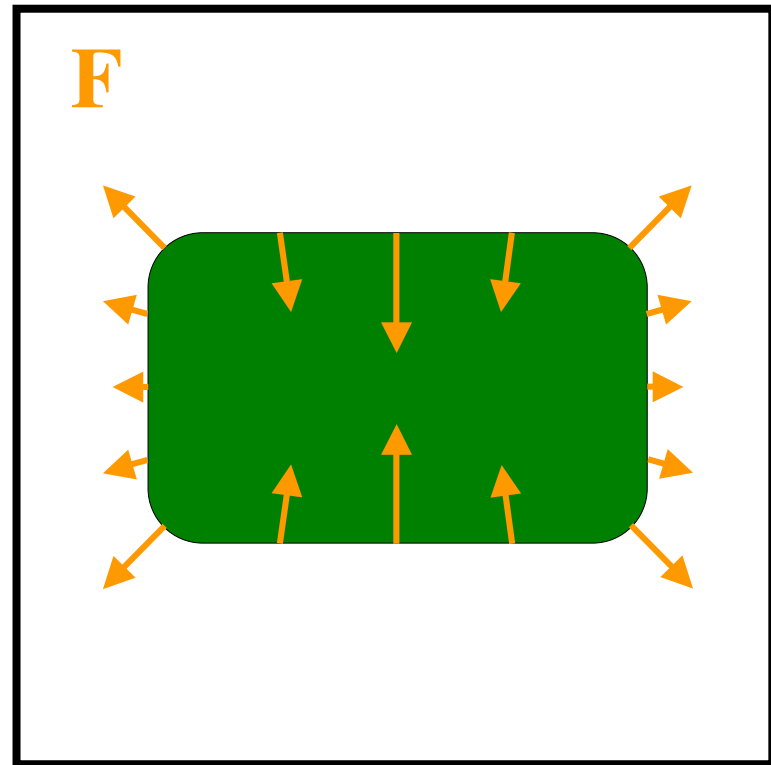


High-dim. registration

Continuum mechanics registration



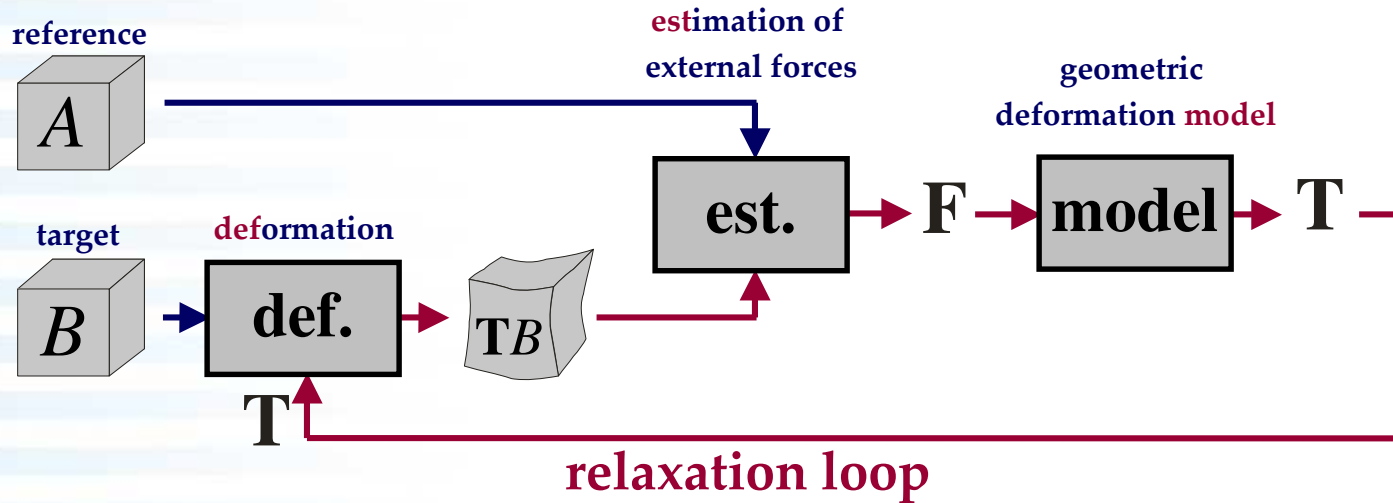
reference A



registered TB



High-dim. registration



Transformation is given as voxel displacements.

Ext. forces tend to maximize image similarity.

Geometric deformation model maps the ext. forces into a new (improved) transformation.

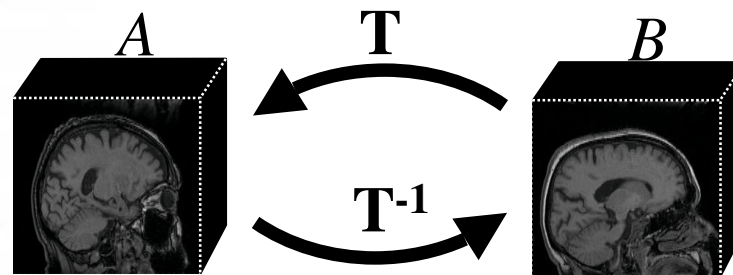


External forces

- Obtained as gradients of image similarity with respect to transformation:

$$F = \frac{\partial S(A, TB)}{\partial T}$$

Similarity measurement is asymmetric...



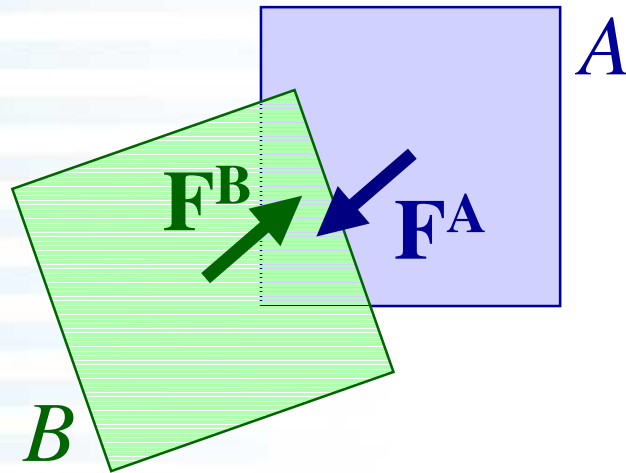
$$S(A, TB) \neq S(T^{-1}A, B)$$

...leading to inverse inconsistency of registration!

Proposed solution: “Symmetric image registration”.



Symmetric reg. approach



Images are treated equally.

External forces are computed for both images and act between the images.

Newton's 3rd law of motion (action reaction):

$$\mathbf{F}^A = -\mathbf{F}^B$$

The forces are symmetric!



Similarity metrics

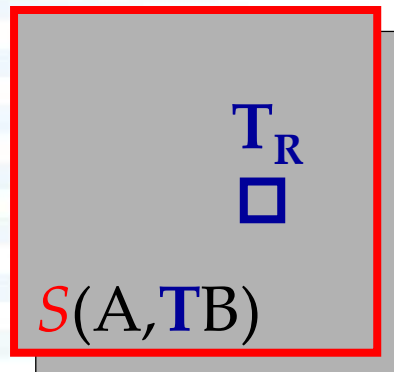
- ♦ **Mono-modality:**
 - ♦ MSD (mean square distance)
 - ♦ CC (correlation coefficient)
- ♦ **Multi-modality**
 - ♦ MI (mutual information)
 - ♦ NMI (normalised mutual information)



Multi-modality and locality

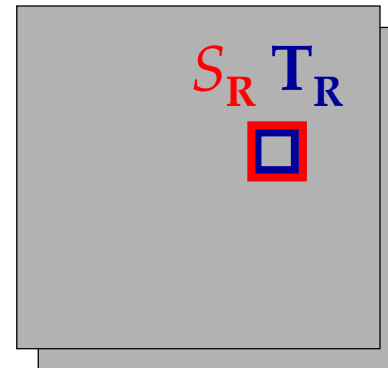
Detection of local image discrepancies:

Measuring global similarity:



High computational cost
in practice limits the
dimensionality and
registration precision.

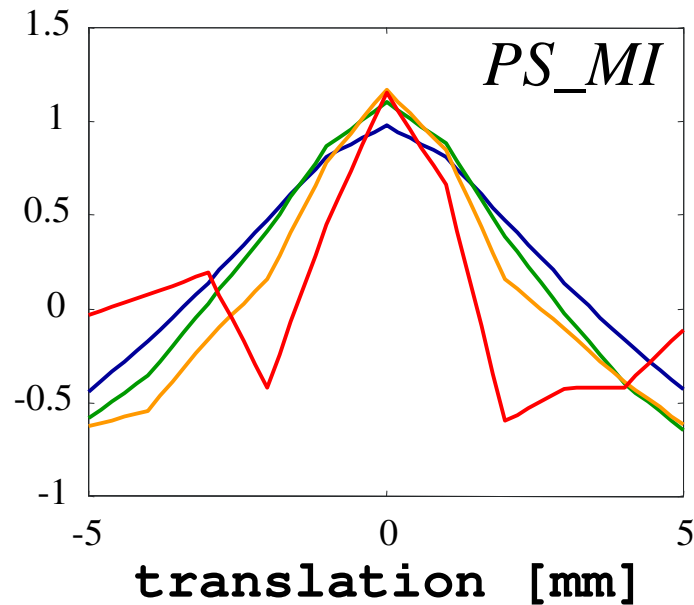
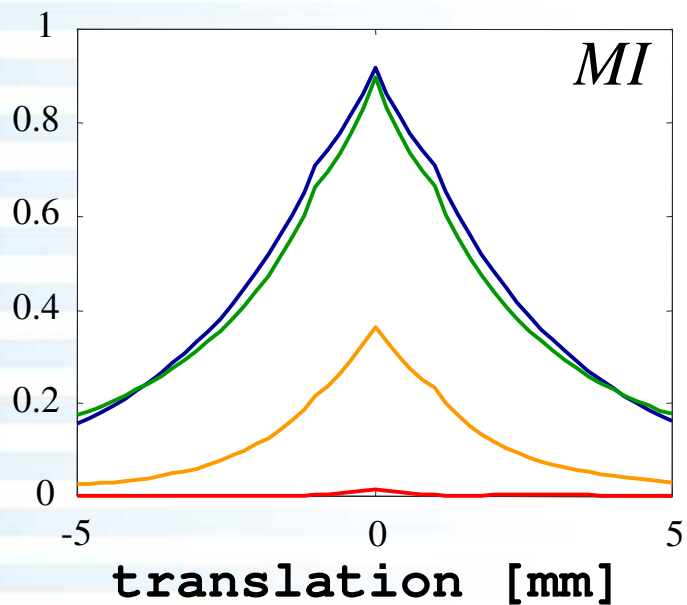
Measuring local similarities



Statistical multi-modality
similarity measures are limited
to large image regions.



Locality and multi-modality



Region size:

- $r = 50$
- $r = 20$
- $r = 10$
- $r = 5$

Proposed solution: “point similarity measures”.

PS_MI : point similarity measure based on MI



Point similarity measures

Procedure, MI example:

- ♦ Global estimation of intensity dependance between images:

$$f_{MI}(\mathbf{i}) = \log \frac{p(\mathbf{i})}{p(i_A)p(i_B)}$$

- ♦ Local (point) similarity measurement

$$S_{MI}(\mathbf{x}_1, \mathbf{x}_2) = f_{MI}(\mathbf{i}(\mathbf{x}_1, \mathbf{x}_2))$$

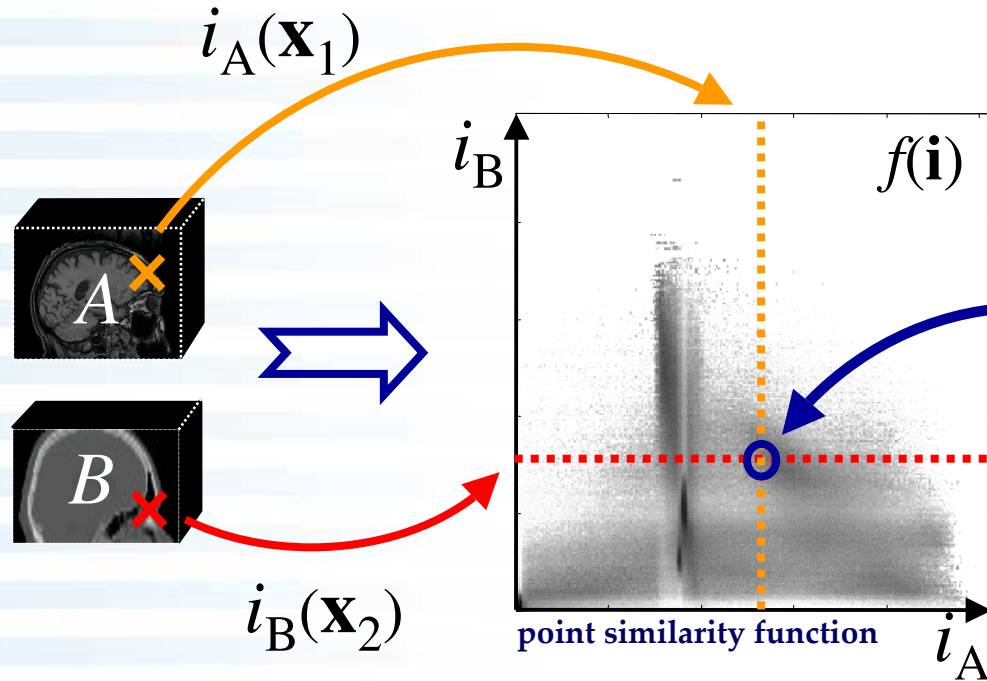
- ♦ Eventual averaging (locality dependent)

$$MI = \overline{S_{MI}(\mathbf{x})}$$



Point similarity measures

Procedure, MI example: $f_{MI}(\mathbf{i}) = \log \frac{p(\mathbf{i})}{p(i_A)p(i_B)}$



Similarity of points:

$$f_{MI}(i_A, i_B) = S_{MI}(\mathbf{x}_1, \mathbf{x}_2)$$

Similarity of a region:

$$S_R = \overline{S_{MI}(\mathbf{x}, \mathbf{x})} \Big|_{\mathbf{x} \in R}$$

Similarity of whole images: $MI = \overline{S_{MI}(\mathbf{x}, \mathbf{x})}$



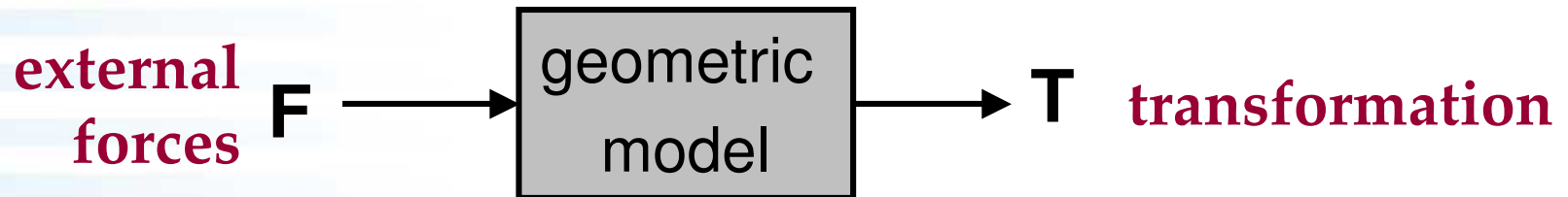
Benefits

- ♦ **Locality**
(also for multi-modality measures)
- ♦ **Low computational cost**
(similarity function serves as a LUT)
- ♦ **Solution to interpolation artefacts**
(when using interpolation of similarity).
- ♦ **Accuracy and robustness**
(variety of methods for computing similarity functions)
- ♦ **Ability to use prior knowledge**
(prior knowledge in intensity domain)
- ♦ ...



Geometric models

- ♦ Geometric models define the space of admissible transformations (deformations).
- ♦ In the case of high dimensional registration they define the relationship between external forces and consequent transformation.



- ♦ Because image deformation should follow deformation of real objects/tissues, physical deformation properties are often used, e.g., **elasticity, viscosity...**



Realistic def. models

- ♦ **Sources of unrealism:**
 - ♦ Simplifications of physical deformation properties and usage of unrealistic models.
 - ♦ Usage of homogenous deformation models.
 - ♦ External forces (obtained as gradients of image similarity) are not realistic!
- ♦ **Realistic models may not be optimal!**



Geometric models

Implementations:

- ♦ **Solution of elastic PDE** (Broit and Bajcsy, 1981)
- ♦ **Finite-element method** (Gee et al., 1994)
- ♦ **Elastic convolution kernel** (Bro-Nielsen, Gramkow 1996)
- ♦ **Simplifications: separable kernels, e.g. Gaussian.**
- ♦ **Important physical characteristics may be obtained by additional constraints (e.g., volume preservation...)**
- ♦ **Inhomogeneous models (different tissues modeled differently, with different properties or different models)**

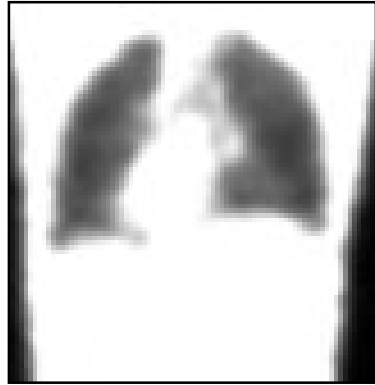


Examples (1)

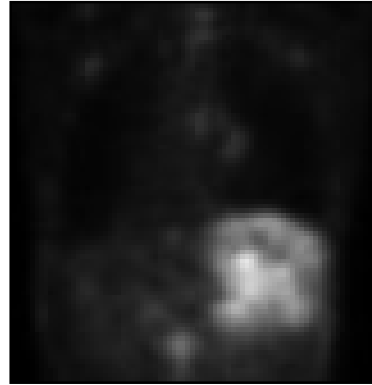
CT / PET image fusion:



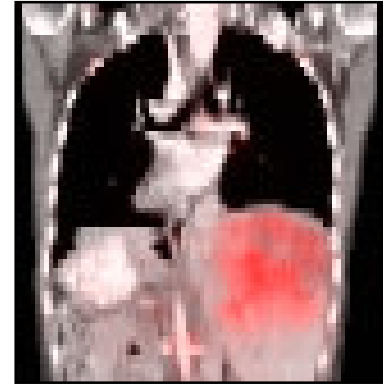
CT



PET-tr



PET-em

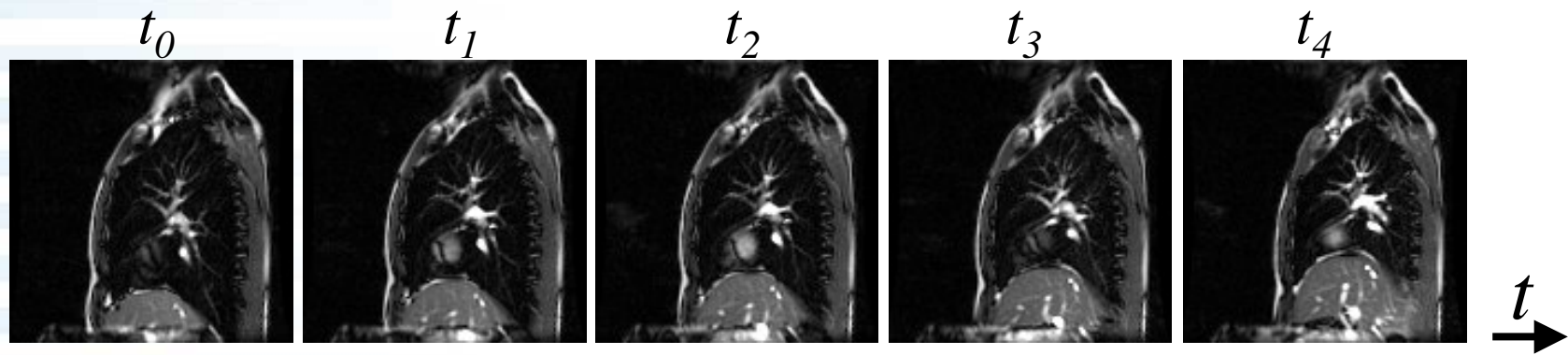


**combined
CT and PET-em**

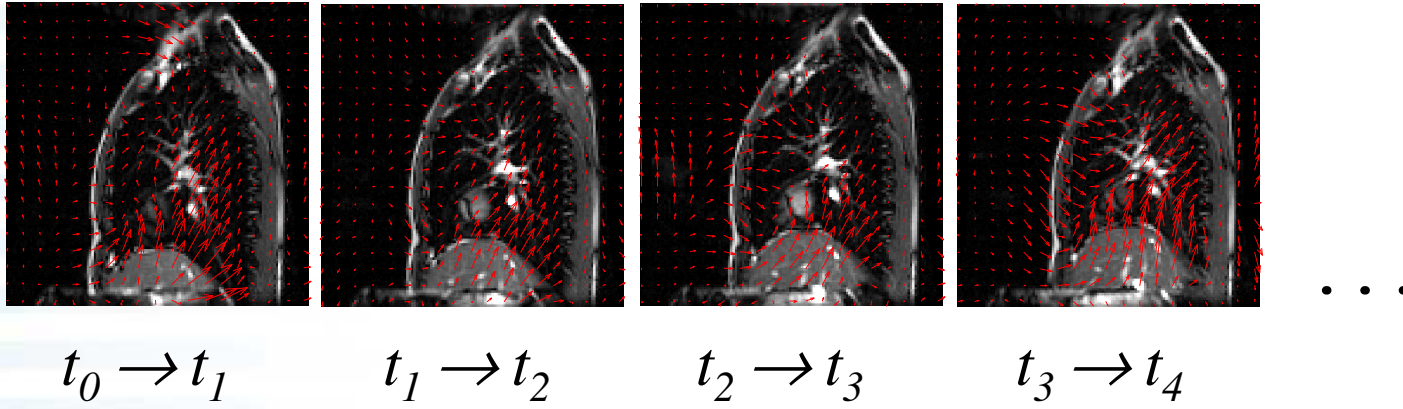


Examples (2)

Breathing motion analysis



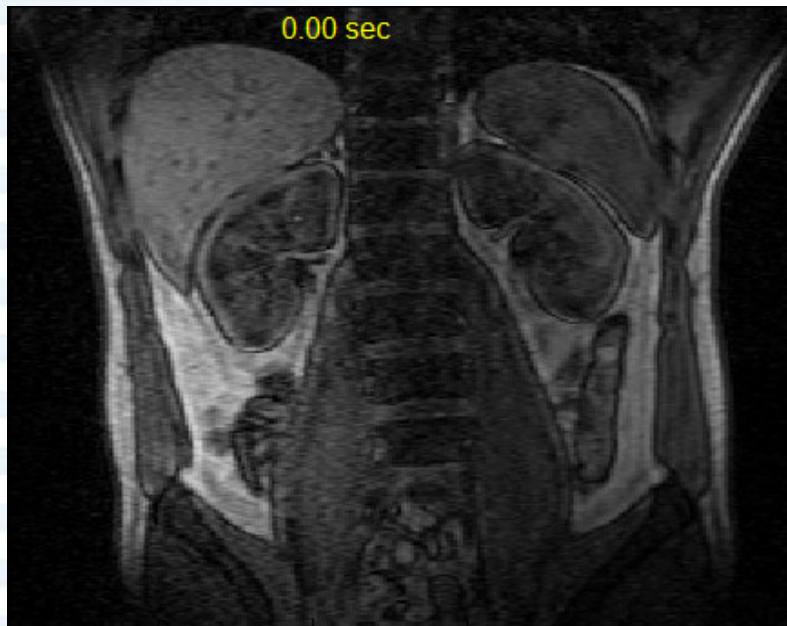
estimated
motion



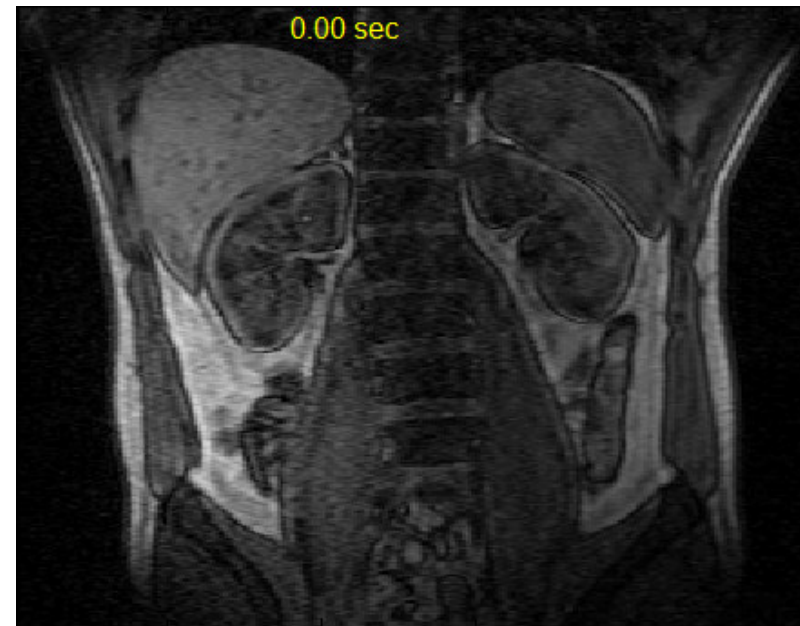


Examples (3)

Registration of kidney time series



original



registered

A collaborative work related to the Kidney MRI project at University of Bergen



Conclusion

- ♦ **Medical image registration can contribute to a broad range of medical procedures**, e.g., to medical diagnostics, treatment planning, surgeries, radiotherapy...
- ♦ **The interest of medicine is increasing.**
- ♦ **Lots of possibilities for improving registration** by integrating prior knowledge, i.e., anatomical knowledge and knowledge related to image formation.

<http://vision.fe.uni-lj.si>



Papers:

Symmetric image registration:

- Peter Rogelj, Stanislav Kovačič. "Symmetric Image Registration". *Medical Image Analysis*, 10(3): 484-493, June 2006.

Point similarity measures:

- Peter Rogelj, Stanislav Kovačič, James C. Gee. "Point similarity measures for non-rigid registration of multi-modal data". *Computer Vision and Image Understanding*, 92(1): 112-140, October 2003.
- Peter Rogelj, Stanislav Kovačič. "Point similarity measure based on mutual information". In: James C. Gee, J. B. Antoine Maintz, Michael W. Vannier (eds.), *Biomedical Image Registration : revised papers*, (Lecture notes in computer science, vol.2717), pp.112-121. Springer-Verlag, June 2003.
- Peter Rogelj, Stanislav Kovačič. "Rigid multi-modality registration of medical images using point similarity measures". In: O. Drbohlav (ed.), *Proceedings of the 8th Computer Vision Winter Workshop CVWW'03*, pp.159-163. February 2003.

Deformation models:

- Peter Rogelj, Stanislav Kovačič. "Spatial deformation models for non-rigid image registration". *CVWW'04*, pp.79-88, February 2004.

<http://vision.fe.uni-lj.si>